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Andressa Borin Venturini

EFEITO DA CONCENTRAÇÃO DE ÁCIDO FLUORÍDRICO NA CARGA PARA FALHA EM FADIGA DE UMA CERÂMICA FELDSPÁTICA CIMENTADA

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Tese apresentada ao Curso de Doutorado do Programa de Pós-Graduação em Ciências Odontológicas, Área de Concentração em Odontologia, ênfase em Prótese Dentária, da Universidade Federal de Santa Maria (UFSM, RS), como requisito parcial para obtenção do título de **Doutor em Ciências Odontológicas**.

Orientador: Prof. Dr. Luiz Felipe Valandro

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"Somos todos anjos de uma asa só, e somente podemos voar quando abraçados uns aos outros."
Lucíano de Crescenzo

RESUMO

EFEITO DA CONCENTRAÇÃO DE ÁCIDO FLUORÍDRICO NA CARGA PARA FALHA EM FADIGA DE UMA CERÂMICA FELDSPÁTICA CIMENTADA

AUTORA: Andressa Borin Venturini ORIENTADOR: Luiz Felipe Valandro

A presente tese é composta por dois artigos científicos que avaliaram a influência de diferentes concentrações de ácido fluorídrico na carga para falha em fadiga de coroas e discos de cerâmica feldspática cimentados à um material análogo a dentina (resina epóxi). Para tanto, oitenta coroas com geometria simplificada e oitenta discos de cerâmica feldspática (Vita Mark II, Vita Zahnfabrik) foram divididos aleatoriamente, e a superfície interna de cada coroa/disco foi tratada de acordo com um dos quatro métodos de condicionamento de superfície (n=20): sem condicionamento/controle (CTRL), ou condicionamento por 60 s com diferentes concentrações de ácido fluorídrico: 1% (HF1), 5% (HF5) ou 10% (HF10). A superfície cerâmica tratada recebeu a aplicação de um agente de união silano. A superfície de cimentação dos preparos para coroas totais simplificadas e dos discos (ambos em resina epóxi) foram condicionados com ácido fluorídrico 10% por 60 s seguido da aplicação de uma camada de adesivo específico do sistema de cimentação. Após os tratamentos de superfície, as coroas e discos cerâmicos foram cimentados adesivamente aos respectivos preparos protéticos e discos de resina epóxi, os quais foram submetidos a cargas cíclicas em água pelo método da escada (500.000 ciclos, 20 Hz). Os dados de carga para falha em fadiga foram analisados pela análise de variância (ANOVA-1 fator) e testes de Tukey (α=0,05). Para as coroas cerâmicas, as cargas médias para falha em fadiga dos grupos CTRL (245,0 \pm 15,1 N), HF1 (242,5 \pm 24,7 N) e HF10 (255,7 \pm 53,8 N) foram estatisticamente semelhantes (P>0,05), enquanto que a carga média do grupo HF5 (216,7 ± 22,5 N) foi significativamente inferior. Na condição de discos cimentados, a carga de falha média do grupo HF5 (255,0 ± 23,0 N) também foi significativamente inferior; o grupo HF1 (301,7 \pm 71,0 N) apresentou valores intermediários e os valores mais altos foram alcançados nos grupos CTRL (351,7 ± 13,4 N) e HF10 (341,7 ± 20,6 N). O condicionamento com ácido fluorídrico 5% teve um efeito deletério nos valores de carga para falha em fadiga de coroas e discos de cerâmica feldspática cimentados adesivamente, visto que o condicionamento com ácido fluorídrico 10% não teve influência negativa em ambas as condições testadas (coroas e discos).

Palavras-chave: Ácido Fluorídrico. Carregamento Cíclico. Cerâmica Feldspática. Fadiga. Tratamento de superfície.

ABSTRACT

EFFECT OF HYDROFLUORIC ACID CONCENTRATION ON THE FATIGUE FAILURE LOAD OF A CEMENTED FELDSPATHIC CERAMIC

AUTHOR: Andressa Borin Venturini ADVISOR: Luiz Felipe Valandro

The present thesis is composed by two scientific articles that evaluated the influence of different hydrofluoric acid concentrations on the fatigue failure loads of feldspathic ceramic crowns and discs adhesively cemented to a dentin analogue material (epoxy resin). Therefore, eighty crowns with simplified geometry and eighty feldspathic ceramic discs (Vita Mark II, Vita Zahnfabrik) were randomly allocated, and the intaglio surface of each crown/disc was treated with one of the four surface conditioning methods (n=20): nonetched / control (CTRL), or etched for 60 s with different hydrofluoric acid concentrations: 1% (HF1), 5% (HF5), or 10% (HF10). The treated ceramic surface received the application of a silane coupling agent. The cementation surface of simplified complete crown preparations and discs (both in epoxy resin) were etched with 10% hydrofluoric acid for 60 s and received a primer coating specific to the cementation system. After the surface treatments, the ceramic crowns and discs were adhesively cemented to the respective prosthetic preparations and epoxy resin discs, which were subjected to cyclic loads in water by a staircase approach (500,000 cycles, 20 Hz). Fatigue failure load data were analyzed by 1-way ANOVA and Tukey's tests (α= .05). For the ceramic crowns, mean failure loads of groups CTRL (245.0 \pm 15.1 N), HF1 $(242.5 \pm 24.7 \text{ N})$ and HF10 $(255.7 \pm 53.8 \text{ N})$ were statistically similar (P>.05), while the mean load of the HF5 group (216.7 \pm 22.5 N) was significantly lower. In the condition of cemented discs, mean failure load of the HF5 group (255.0 \pm 23.0 N) was also significantly lower; HF1 group (301.7 \pm 71.0 N) presented intermediate values, and the highest values were achieved in CTRL (351.7 \pm 13.4 N) and HF10 (341.7 \pm 20.6 N) groups. Etching with 5% hydrofluoric acid had a deleterious effect on the fatigue failure loads of adhesively cemented feldspathic ceramic crowns and discs, while etching with 10% hydrofluoric acid had no negative influence in both tested conditions (crowns and discs).

Keywords: Cyclic Loading. Fatigue. Feldspathic Ceramic. Hydrofluoric Acid. Surface treatment.

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1 INTRODUÇÃO

As cerâmicas têm ganhado papel de destaque na Odontologia Restauradora por satisfazerem a crescente exigência estética dos pacientes (KELLY, 2004), pelo desenvolvimento de materiais mais confiáveis e utilização de sistemas CAD/CAM (Computer Aided Design/Computer Aided Machine). A longevidade clínica das restaurações totalmente cerâmicas é dependente de uma combinação de fatores, tais como a durabilidade da união adesiva, a confiabilidade mecânica do material cerâmico (GUESS et al., 2009), e as cargas cíclicas às quais os materiais são submetidos quando em função (ZHANG et al., 2006).

Os blocos cerâmicos pré-fabricados para usinagem em sistemas CAD/CAM (Computer Aided Design/Computer Aided Machine) são confeccionados sob condições industriais padronizadas e reproduzíveis, consistindo em um material mais confiável estruturalmente e homogêneo devido a menores chances de incorporação de defeitos e poros (GIORDANO, 2006). Dentre os blocos cerâmicos disponíveis, Vitablocs Mark II (Vita Zahnfabrik, BadSäckingen, Alemanha) são produzidos com uma cerâmica de estrutura feldspática fina, e indicados para confecção de facetas, inlays/onlays, coroas anteriores e posteriores (VITA ZAHNFABRIK, 2012). Embora esse material apresente uma resistência flexural relativamente baixa de aproximadamente 86 MPa, possui elevado módulo de Weibull (m=23,6) (TINSCHERT et al., 2000). Clinicamente, coroas monolíticas de Vita Mark II apresentam taxas de sobrevivência semelhante às coroas com infraestrutura de Vita In Ceram Spinell em um período 2 a 5 anos (BINDL; MÖRMANN, 2004). Além disso, essas coroas (Vita Mark II) são significativamente reforçadas por procedimentos adesivos adequados (BINDL; LÜTHY; MÖRMANN, 2006).

Nesse sentido, a qualidade da união estabelecida entre cerâmica e cimento é um fator que pode afetar a resistência à fratura de restaurações cerâmicas (BINDL; LÜTHY, H.; MÖRMANN, 2006). Estudos que compararam cimentação adesiva e convencional demonstraram que coroas cimentadas adesivamente suportaram cargas mais altas para fratura (MÖRMANN et al., 1998; BINDL; LÜTHY; MÖRMANN, 2006). Em um estudo clínico de sobrevivência de coroas cerâmicas vítreas (Dicor), Malament e Socranski (2001) observaram que as coroas submetidas ao condicionamento ácido, previamente à cimentação, tiveram maior probabilidade de sobrevivência (75%) quando comparadas àquelas sem condicionamento (43%), em um período superior a 16 anos.

O processo adesivo das cerâmicas baseadas em sílica (vítreas) aos cimentos resinosos parece estar bem estabelecido, visto que a união é proporcionada pelo condicionamento com

ácido fluorídrico (HORN, 1983) e potencializada pelo agente de união silano (BRENTEL et al., 2007). O condicionamento com ácido fluorídrico, realizado na superfície interna da peça cerâmica, ataca seletivamente a fase vítrea das cerâmicas, expondo óxidos de sílica (SiO₂), e produzindo alterações topográficas que contribuem para a retenção micromecânica a materiais resinosos (PHOENIX; SHEN, 1995; ROULET; DEGRANGE, 1996; THORDRUP et al., 1999). Esse condicionamento ácido modifica a superfície cerâmica em função da concentração de ácido fluorídrico utilizado e do tempo de condicionamento (ADDISON; MARQUIS; FLEMING, 2007b). Entretanto, grande parte das tensões de tração, responsáveis pelo início da falha em coroas cerâmicas, concentram-se na superfície de cimentação da peça cerâmica, na qual o procedimento de condicionamento ácido é realizado (KELLY et al., 1990; THOMPSON et al., 1994; QUINN et al., 2005; MAY et al., 2012).

Embora o condicionamento com ácido fluorídrico promova a rugosidade de superfície necessária para criar retenção micromecânica, estudos *in vitro* têm relatado que esse procedimento poderia enfraquecer o material cerâmico (ADDISON; FLEMING, 2004; ADDISON; MARQUIS; FLEMING, 2007b; HOOSHMAND; PARVIZI; KESHVAD, 2008; VENTURINI et al., 2015b). Em contrapartida, o condicionamento com ácido fluorídrico não afetou a resistência à fratura de cerâmicas vítreas quando um procedimento adesivo foi empregado após o condicionamento da superfície (YEN et al., 1993; PAGNIANO et al., 2005; POSRITONG, et al., 2013). Além disso, esse ácido também é conhecido como um produto químico com efeitos extremamente perigosos devido à sua toxicidade (OZCAN; ALLAHBEICKARAGHI; DUNDAR, 2012), o que tem motivado pesquisadores a testar concentrações mais baixas de ácido fluorídrico.

Os estudos laboratoriais (YEN et al., 1993; ADDISON; FLEMING, 2004; PAGNIANO et al., 2005; ADDISON; MARQUIS; FLEMING, 2007b; HOOSHMAND; PARVIZI; KESHVAD, 2008; POSRITONG, et al., 2013; VENTURINI et al., 2015b) que avaliaram o efeito de diferentes regimes de condicionamento (tempo e concentração de ácido fluorídrico) na resistência flexural de cerâmicas vítreas utilizaram testes monotônicos com espécimes na forma de barras ou discos. Testes monotônicos consistem na aplicação única de carga crescente até a fratura do corpo de prova, e são amplamente utilizados para a caracterização de materiais e avaliação da influência de variáveis nas propriedades mecânicas. Desta forma, os materiais não falham devido a um dano cumulativo (fadiga), como ocorre quando os materiais estão em função (SCHERRER et al., 2003). Em contrapartida, os ensaios de fadiga cíclica são testes complementares aos ensaios monotônicos tradicionais, pois reproduzem uma condição mais próxima ao cenário clínico (WISKOTT; NICHOLLS;

BELSER, 1995; MAY et al., 2015). Um dos ensaios baseados na aplicação de carga cíclica é o método da escada ("staircase method" ou "up and down method") que estabelece a resistência à fadiga do material (valor de tensão em que a falha ocorrerá após um tempo de vida específico). Nesse método, um número de ciclos é pré-determinado para aplicação de uma carga inicial de magnitude inferior à tensão máxima suportada pelo material e, dependendo da ocorrência ou não de fratura, a carga é aumentada ou diminuída, empregandose um incremento fixo nas fases seguintes (COLLINS, 1993).

Portanto, os estudos laboratoriais citados anteriormente além de utilizarem apenas ensaios monotônicos, não levaram em consideração a influência da geometria da restauração na distribuição de tensões, nem o método de confecção dos corpos-de-prova (KELLY, 1999). Além disso, os procedimentos de cimentação e o suporte dentinário (módulo de elasticidade da dentina) não foram considerados na maioria desses estudos. Até o presente momento, não há estudos na literatura que tenham avaliado a influência de diferentes concentrações de ácido fluorídrico em espécimes de cerâmica feldspática cimentados adesivamente e submetidos a ensaios de fadiga cíclica, cujo contexto de teste apresenta maior relevância clínica.

Ainda no sentido da influência da geometria da restauração, alguns estudos (MAY et al., 2012; ANAMI et al., 2015) validaram ensaios com espécimes em forma de coroas simplificadas, que dispensam o uso de uma completa anatomização oclusal para avaliar desfechos clínicos. Em relação à facilidade metodológica, Chen et al. (2014) utilizaram uma metodologia de ensaio simplificada para simulação de restaurações em dentes posteriores, no qual discos cerâmicos são cimentados adesivamente a discos de um substrato análogo a dentina obtendo-se uma espessura final de 3,5 mm, equivalente à espessura média da parede pulpar à superfície oclusal. Entretanto, comparações sobre a eficácia de simulação desse método simplificado (disco sobre disco proposto por Chen) em relação ao uso de restaurações na forma de coroas cimentadas não foram investigadas.

A fim de prever de maneira mais confiável o comportamento mecânico da superfície cerâmica após os procedimentos de condicionamento com ácido fluorídrico e cimentação, espécimes na forma de coroas e discos de cerâmica feldspática foram submetidos a ensaios de fadiga cíclica em meio úmido. Por consequência, fatores como a distribuição de tensões, propagação de trincas, e a interação da população de defeitos da cerâmica com o cimento resinoso serão mais semelhantes à situação encontrada clinicamente. Portanto, o presente trabalho visa avaliar, através do método de "staircase", o impacto do condicionamento com ácido fluorídrico e suas diferentes concentrações na carga para falha em fadiga de coroas e de discos de cerâmica feldspática cimentados adesivamente a um material análogo a dentina.

2 ARTIGO 1 – FATIGUE FAILURE LOAD OF FELDSPATHIC CERAMIC CROWNS AFTER HYDROFLUORIC ACID ETCHING AT DIFFERENT CONCENTRATIONS

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Fatigue failure load of feldspathic ceramic crowns after hydrofluoric acid etching at different concentrations

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Fatigue failure load of feldspathic ceramic crowns after hydrofluoric acid etching at different concentrations

ABSTRACT

Statement of problem: Hydrofluoric acid etching modifies the cementation surface of ceramic restorations, which is the same surface where failure is initiated. Information regarding the influence of hydrofluoric acid etching on the cyclic loads to failure of ceramic crowns is lacking. **Purpose:** The purpose of this in vitro study was to evaluate the influence of different hydrofluoric acid concentrations on the fatigue failure loads of feldspathic ceramic crowns. Materials and Methods: Eighty feldspathic ceramic crowns were cemented with resin cement to identical simplified complete crown preparations machined in a dentinlike polymer. The preparations were etched with 10% hydrofluoric acid for 60 seconds and received a primer coating. Before cementation, the intaglio of the ceramic crowns was treated with 1 of 4 surface conditionings (n=20): nonconditioned (control, CTRL), or etched for 60 seconds with different hydrofluoric acid concentrations: 1% (HF1), 5% (HF5), and 10% (HF10). A silane coupling agent was applied on this surface of all crowns, which were cemented to the preparations. Each crown was cyclically loaded in water with a G10 epoxyglass piston positioned in the center of the occlusal surface. Fatigue failure loads of ceramic crowns were obtained by the staircase approach after 500 000 cycles at 20 Hz. Mean failure loads were analyzed by 1-way ANOVA and the Tukey test (α =.05). **Results:** Mean failure loads of groups CTRL (245.0 ±15.1 N), HF1 (242.5 ±24.7 N), and HF10 (255.7 ±53.8 N) were statistically similar (P>.05), while that of the HF5 group (216.7 ±22.5 N) was significantly lower (P<.05). **Conclusion:** HF5 acid had a negative effect on the fatigue loads of the tested feldspathic ceramic crowns, while HF1 and HF10 acids did not change the fatigue resistance.

Clinical Implications

Hydrofluoric acid etching does not have a weakening effect on resin-bonded feldspathic ceramic crowns. However, the clinical use of 5% hydrofluoric acid for etching this ceramic should be considered carefully.

1. INTRODUCTION

The long-term success of ceramic restorations is determined by the durability of the adhesive bond and by the mechanical reliability of the ceramic material. Ceramic restorations are constantly subjected to cyclic loads in wet conditions, and the combination of these factors has been identified as one of the main causes of crack initiation and subsequent growth, which may decrease the strength and increase the failure of the restorative materials. ^{2,3}

Vitablocs Mark II (Vita Zahnfabrik) are fine-structure feldspar ceramic blocks used to produce inlays, onlays, veneers, and crowns with computer-aided design and computer-aided manufacturing (CAD-CAM) systems. Industrially prepared ceramic blocks are more structurally reliable materials for dental applications, although the machining process may induce flaws.⁴ Vita Mark II has a relatively low flexural strength of 86.3 MPa, but it has a high Weibull modulus (m=23.6).⁴ Clinically, complete crowns of Vita Mark II showed similar survival rates to crowns with Vita In-Ceram Spinell copings over a period of 2 to 5 years.⁵ Furthermore, appropriate bonding procedures can improve not only the bond strength but also the fracture strength of CAD-CAM crowns.⁶

During the bonding procedure, the intaglio surface of feldspathic ceramic restorations should be etched with hydrofluoric acid to provide the necessary surface alterations and surface roughness for mechanical interlocking.⁷ These surfaces are further primed with a silane coupling agent for chemical bonding of the ceramic, silane, and resin cement.^{7,8} The experimental evaluation of clinically failed complete ceramic crowns and finite element analysis results suggests that the majority of bulk fractures of single-unit crowns are initiated from the intaglio of the ceramic (cementation surface), where high tensile stresses develop during cyclic loading^{2,9-13} and where hydrofluoric acid etching is performed. Therefore, the

internal surface characteristics of ceramic crowns are believed to play a crucial role in their probability of failure.¹⁴

Although hydrofluoric acid etching modifies the intaglio surface of ceramic restorations to promote micromechanical interlocking, the impact of this acid on the ceramic strength remains uncertain. It appears to have a weakening effect on glass ceramics¹⁵⁻¹⁸ because of the modification of the resident surface flaw population,¹⁵ with a progressive increase in this effect as a function of the hydrofluoric acid concentration used for etching.^{16,19} With higher hydrofluoric acid concentrations, the increased number of defects can be attributed to newly introduced flaws.¹⁶ If these flaws reach a critical size, they can propagate on the internal surface and cause ceramic failure. Thus, the flaw distribution present in the material is directly related to the fracture strength of the ceramic.²⁰ However, some studies have reported that hydrofluoric acid in different etching regimens did not negatively impact the strength of ceramics^{21,22} and that unfilled resin or resin cement application had a positive effect on flexural strength after hydrofluoric acid etching and silane treatment,^{14,22} minimizing the influence of flaws.²³ The strengthening effect occurs as a consequence of the interaction of the resin with the entire surface defect population²⁴ and may depend on the behavior of the resin penetrating the ceramic surface.²⁵

In addition, this acid is also known as a chemical with extremely hazardous effects because of its toxicity.²⁶ Therefore, potential damage to health has motivated dental research to test low hydrofluoric acid concentrations.²⁷

The performance of complete ceramic crowns is determined by a complex combination of factors including the material selected, thickness, damage introduced, adhesive/luting system used, tooth substrate (natural dentin or foundation restoration²⁸), and the fatigue response to complex loading.²⁹ In terms of failure prediction, cyclic mechanical loads applied under wet conditions could simulate the damage accumulation that occurs in

ceramic restorations in an oral environment³⁰ and can lead to modes of crack initiation and growth not seen under monotonic loads.³¹ However, the authors are unaware of studies that did not perform monotonic tests to evaluate the effect of hydrofluoric acid etching on the ceramic surface, which can be less clinically relevant than fatigue failure tests. Likewise, the authors are unaware of studies that tested the influence of the restoration geometry on stress distribution or the cementation effects, such as flaw "healing" by resin cement. In addition, the influence of dentin elastic properties and the manufacturing method of the ceramic specimens—related to population defects—need to be studied. Currently, studies that replicated clinical situations that have assessed the influence of hydrofluoric acid etching in different concentrations on the fatigue failure loads of adhesively cemented feldspathic ceramic crowns are lacking.

Therefore, the purpose of this in vitro study was to evaluate the influence of different hydrofluoric acid concentrations on the failure loads of feldspathic ceramic crowns machined by CAD-CAM systems using wet mechanical cyclic tests. Two hypotheses were tested: acid etching would not reduce the fatigue failure loads in comparison with untreated crowns, and mean failure loads would not be influenced by the different hydrofluoric acid concentrations.

2. MATERIAL AND METHODS

The design of a simplified complete crown was adapted from one previously developed by Gressler May et al.³⁰ They observed that fractures were initiated from the cementation surface of feldspathic crowns. Furthermore, the lack of contact damage on the loaded surface was attributed to the use of a flat-end piston made from G10 epoxy glass.

Eighty identical dentin analog prosthetic preparations (preparation height=5.32 mm, internal angle radii=0.5 mm, axial wall convergence=16 degrees, cervical preparation depth=1.2 mm, and round shoulder radii=0.5 mm) were machined from 11 mm diameter rods

of an epoxy-glass cloth (NEMA G10; International Paper) in a mechanical lathe (Diplomat 3001; Nardini), as seen in Figure 1A. One G10 preparation was scanned, and the 3-dimensional images were processed in CAD software (CEREC in-Lab 3D, v4.1; Sirona Dental Systems GmbH) with an occlusal cementation space of 60 µm and an occlusal thickness of 1.5 mm.

A CAM machine (CEREC inLab MC XL; Dentsply Sirona) was used to mill ceramic blocks (10×12×15 mm) (Vita Mark II 4M2C/I12; Vita Zahnfabrik) into identical crowns using diamond rotary instruments and water. Four nominally identical pairs of diamond instruments, each containing 1 cylindrical (Cylinder pointed bur 12S; Dentsply Sirona) and 1 stepped pattern (Step bur 12S; Dentsply Sirona), were used to generate 80 crowns. Each rotary instrument set machined the sample size for each group (n=20). The specimen machining sequence (1 to 20) was recorded for each individual crown, and they were randomly assigned according to the same instrument set using an online tool (http://www.randomizer.org/). After machining, each crown was seated on its respective preparation to evaluate the marginal fit. However, no internal adjustment was needed in the crowns. Nevertheless, their occlusal surface was finished with silicon carbide grit (#600), resulting in a final occlusal thickness of 1.5 ±0.01 mm. The preparations were cleaned in an ultrasonic bath with distilled water for 3 minutes, and the crowns were cleaned with isopropyl alcohol for 5 minutes to remove the polishing residue.

The intaglio surfaces were etched with different hydrofluoric acid concentrations, as summarized in Table 1, for 60 seconds, rinsed with an air-water spray for 30 seconds, dried, and ultrasonically cleaned in distilled water for 5 minutes. Subsequently, the silane-based primer (Monobond Plus; Ivoclar Vivadent AG) was applied on the intaglio of all crowns for 1 minute and then air dried.

The G10 preparations were etched with 10% hydrofluoric acid for 60 seconds, washed for 30 seconds, and ultrasonically cleaned for 5 minutes. Multilink Primer A and B (Ivoclar Vivadent AG) were mixed in a 1:1 ratio, scrubbed on the dies for 30 seconds, and dried until a thin film was obtained.

One centimeter of resin cement (Multilink Automix; Ivoclar Vivadent AG) was measured with a ruler, mixed, and applied to the intaglio crown surface. The crowns were seated under a load of 7.5 N. The excess cement was removed, and the remaining cement was light polymerized with 5 exposures of 20 seconds each.

After the cementation procedures, all specimens, as seen in Figure 1B, were embedded in both polyurethane (F16, Fast Cast Polyurethane; Axson Technologies) and PVC cylinders to 2 mm below the cervical margin. They were then stored in distilled water at 37°C for 7 to 14 days before the staircase load testing was conducted.

Cyclic failure loads were established in an electric machine (Instron ElectroPuls E3000; Instron Corp) using the staircase sensitivity (up and down) approach method described by Collins.³² Each crown was centrally and perpendicularly loaded under water using a 2-mm diameter piston made from G10 epoxy-glass cloth (Fig. 2). A sheet of polyethylene (0.1 mm thick) was placed between the piston and the ceramic to reduce contact stress concentration.

Sinusoidal cyclic loading was applied to ceramic specimens, with amplitudes ranging from a minimum of 10 N to the maximum tensile load, at a frequency of 20 Hz, and for 500 000 cycles. The initial load and the step size were determined based on the results of the monotonic tests from the 10% hydrofluoric acid (HF10) group (n=3; mean monotonic load for fracture=300 N). A load that was 60% of the mean monotonic failure load was assumed as the initial load (180 N). A step size of 20 N was applied up or down to the next specimen, according to the examination for subsurface crack formation by transillumination. If the tested

specimen failed, the next specimen was cycled at a lower load by decreasing 1 step size. If the specimen survived the 500 000 cycles, the subsequent specimen was cycled at a higher load by increasing 1 step size.

The mean failure load (Lf) and the standard deviation (s) were calculated on the basis of the data of the least frequent event (survival or failure) by using the method described by Collins.³²

$$L_f = L_{f0} + d \left[\sum_{i} \ln_i / \sum_{i} n_i \pm 1 / 2 \right]$$
 Eq. (1)

$$s = 1,62d \left\{ \left[\left(\sum n_i \sum i^2 n_i - \left(\left[\sum i n_i \right) \right]^2 \right) / \left(\sum n_i \right)^2 \right] + 0,029 \right\}$$
 Eq. (2)

if:
$$\left[(\sum n_i \sum t^2 n_i - ((\sum t n_i))^2) / (\sum n_i)^2 \right] \ge 0.3$$

where L_{f0} is the lowest load level considered in the analysis, d is the step size, and n_i is the number of failures or survivals at the given load level. In Eq. (2), the negative sign is used if the least frequent event is a failure; otherwise, the positive sign is used. The lowest load level considered is designated as i=0, the next level as i=1, and so on. n_i is the number of failures or survivals at a given load level.

Topographical analysis was performed by field emission scanning electron microscopy (FE-SEM) (FEI Inspect F50; FEI) at different magnifications. For this analysis, a machined crown was sectioned into 4 pieces. Each piece was treated using different conditioning methods, and the occlusal surfaces of cementation (internal surface) were sputter coated with a gold-palladium alloy before being examined.

After the fatigue test, the crowns were analyzed under a light microscope (Stereo Discovery V20; Carl Zeiss) to determine the region of crack origin. Then the failure crowns were longitudinally sectioned into halves perpendicular to the track of the radial crack. Representative specimens from each group were analyzed by FE-SEM.

Statistical analysis was performed using statistical software (IBM SPSS Statistics for Windows v21; IBM Corp). All load values (failure or survival steps) were analyzed by 1-way ANOVA and the post hoc Tukey test (α =.05) because the data presented homogeneity of variances (P>.05 based on the Levene test) and normal distribution (P>.05 based on the Shapiro-Wilk test).

3. RESULTS

Significant differences were found among the groups (ANOVA, P<.001). The crowns etched by 5% hydrofluoric acid (HF5) had a lower mean fatigue failure load than that of the CTRL, 1% hydrofluoric acid (HF1), and HF10 groups, which were statistically similar (Table 2). The patterns of runouts (survivals) and failures from the staircase experimental design for the different groups after 500 000 cycles are shown in Fig. 3.

The FE-SEM analysis revealed that slight topographical changes were promoted by HF1 compared with the untreated condition (CTRL) (Fig. 4). A progressive effect of the different hydrofluoric acid concentrations was observed on the ceramic microstructure, indicating that higher concentrations promoted larger and deeper craters and pits.

The crown failure analysis under a light microscope showed that all fatigue cracks were radial cracks starting from the cemented surface, and there was no Hertzian cone crack. Representative FE-SEM micrographs of the fracture surfaces are presented in Fig. 5. The irregularities created by acid etching on the ceramic surface were often not filled by resin cement, especially in the HF5 group.

4. DISCUSSION

The first hypothesis-that the acid etching would not reduce the fatigue failure loads in comparison with untreated crowns-was partially accepted. Mean fatigue failure loads were

significantly lower when ceramic surfaces were etched with HF5, while the groups CTRL, HF1, and HF10 were not statistically different (Table 2). The second hypothesis was rejected because the fatigue failure loads were influenced by the distinct hydrofluoric acid concentrations.

Malament and Socransky²⁸ reported that the intraoral survival rates (Kaplan-Meier) of glass-ceramic crowns (Dicor) over 16 years were higher when they were acid etched before being bonded to the dentin cores, as opposed to not being acid etched. Of the luting agents tested in that study, acid-etched Dicor restorations luted with composite resin exhibited more favorable survivor functions than restorations luted with glass ionomer or zinc phosphate cement.²⁸ These data highlight the importance of resin-bonded adhesion and topographical changes promoted by hydrofluoric acid etching to achieve better clinical results.

Nevertheless, hydrofluoric acid can be harmful and particularly aggressive to soft tissues. ²⁶ Considering the potential hazards of hydrofluoric acid in dental applications, low concentrations of this acid have been studied to promote durable bond strengths without weakening the ceramics. Venturini et al²⁷ tested 4 hydrofluoric acid concentrations for etching a feldspathic ceramic (Vita Mark II), concluding that 3%, 5%, and 10% hydrofluoric acid promoted stable resin adhesion after long-term aging, while 1% hydrofluoric acid showed a significant decrease in bond strength after aging/thermocycling. In another study, ¹⁸ they tested the effect of the same hydrofluoric acid concentrations on the flexural strength and reported that acid etching has a weakening effect on feldspathic ceramic when compared with untreated ceramic, regardless of its concentration. Regardless of these previous monotonic findings, the mean fatigue failure loads were not different among the groups CTRL, HF1, and HF10 in the current study. The explanation for this could be the cementation procedure, which provides support to the ceramic crown by a cement layer. A positive influence of the resin cement application on the ceramic flexural strength has been proposed by some

authors.^{22,24,25} The theory of resin strengthening ceramics may be explained by the combination of the Poisson constraint and the creation of a resin interpenetrating layer sensitive to the elastic modulus of the resin.²⁵ A resin layer that is bonded to the flawed surface would change the ceramic material to a ceramic-composite resin.¹²

Etching the cementation surface and bonding with a low-viscosity resin cement can minimize the influence of flaws at cementation surfaces.²³ However, crowns etched with 5% hydrofluoric acid were significantly less resistant than the other groups tested here. The FE-SEM fractography images (Fig. 5) show nonhomogeneous penetration of the resin cement into the ceramic irregularities created by 5% hydrofluoric acid through the cement voids present at the interface, mainly in the failure origin area. The presence of a large flaw and cement voids along the internal surface of a glass-ceramic crown may raise internal stresses, leading to failure.¹² Under loading, the stress at the flaw tip in an air space cannot be transferred to the resin, thereby increasing the susceptibility of the ceramic to crack initiation.¹² The resin cement viscosity is also important, as more fluid resin cement could penetrate irregularities on the intaglio ceramic surface.

Previous investigations of clinically failed glass-ceramic crowns revealed that the majority of failures were initiated from flaws and tensions existing at the cementation surface, indicating this surface as the location of the highest tensile stress and/or the largest flaws. ^{9,11,13} In the current study, all failures occurred as radial cracks from the cementation surface, which approximate to the clinical failure reports. In addition, the use of a flat-end piston made from G10 epoxy glass and a plastic strip between the piston and the crown during the test may justify the absence of contact damage on the loaded occlusal surface.

The load to initiate a radial fracture is influenced by the crown thickness and the relative elastic modulus between crown and the supporting tooth substrate.²⁹ Hence, the current study used a crown design with a simple geometric configuration because an irregular

geometry makes it difficult to determine the effect of crown thickness. In addition, the substrate supporting material was an epoxy filled with woven glass fibers (G10), which has an elastic modulus similar to that of dentin. Kelly et al¹⁰ reported that G10 was not significantly different from hydrated dentin in terms of blunt contact elastic behavior or resin cement bond strength. They found a small difference (approximately 5%) in fatigue behavior when testing was performed at 20 Hz versus 2 Hz and concluded that further tests can be performed at 20 Hz, greatly increasing the rate of data accumulation. Therefore, the current fatigue test was performed at 20 Hz.

Regarding the fatigue test, the staircase approach was used to determine the fatigue strength; it involved subjecting specimens to a high number of cycles at a low load. At least 15 specimens were necessary to evaluate the fatigue strength at the life of interest.³² Coefficients of variation of approximately 10% were achieved by Kelly et al,¹⁰ with a modest number of specimens (\leq 20) in a staircase sensitivity testing. Because of its low variability, a sample size of 20 crowns was used in the present study.

There are limitations in this in vitro study, and some clinical conditions were not simulated. The direction of the load application was only axial, without simulation of lateral forces and sliding that may occur clinically during mastication or clenching. Furthermore, the brief water storage times (7 to 14 days), without long-term aging, might be insufficient to damage bond strength. The chemical bond between silane and resin cement might deteriorate over time because of hydrolysis, and the micromechanical retention promoted by the minimal acid etching (HF1) or nonacid etching (CTRL) may be insufficient to provide stable bond strength. Therefore, the adhesion in CTRL and HF1 may have been promoted mainly by chemical bonds, with minimum micromechanical bonding. Thus, these findings should be considered carefully, and future studies should stress the clinical plausibility of using lower concentrations of hydrofluoric acid.

5. CONCLUSIONS

Within the limitations of this in vitro study, the following conclusions were drawn:

- 1. Etching with 5% hydrofluoric acid on the intaglio surface of feldspathic ceramic crowns reduced the fatigue failure loads and thus would not be recommended for the tested ceramic.
- 2. The mean fatigue failure loads of the feldspathic crowns was not influenced by 1% and 10% hydrofluoric acid, since these etched crowns did not differ from untreated crowns.

ACKNOWLEDGMENTS

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FIGURES

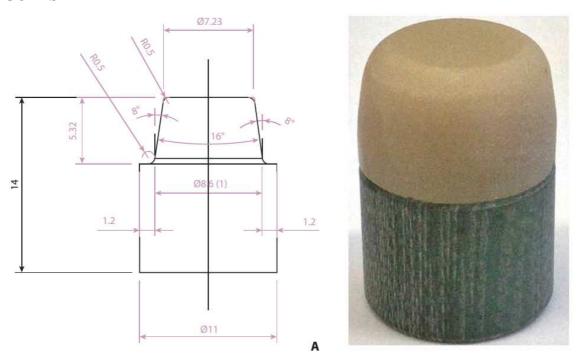


Figure 1. Illustrations of a G10 preparation for crown cementation. A, Sketch lines and dimensions (in mm) for the axial-symmetric drawing of the G10 preparation. B, Specimen after crown cementation.



A B

Figure 2. Experimental arrangement. Specimen centrally loaded with G10 piston in fatigue machine.

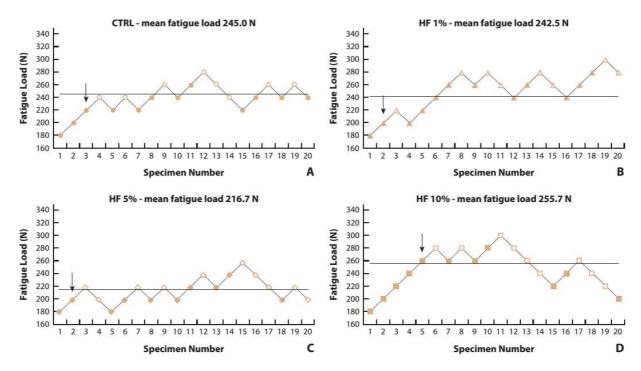


Figure 3. Pattern of runouts (survival) and failures for each group (CTRL, HF1, HF5, HF10) observed during wet mechanical cycling (500 000 cycles). Arrows indicate load level at which up-and-down character started. Horizontal lines indicate mean fatigue load, filled scorers show runout, and empty scorers are failure.

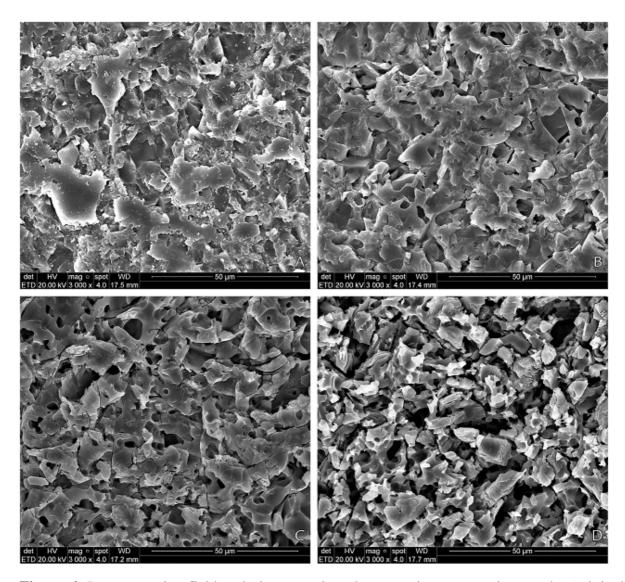


Figure 4. Representative field emission scanning electron microscopy micrographs (original magnification, ×3000) of different ceramic surface treatments showing topography pattern alteration generated by machining procedure and hydrofluoric acid etching. A, CTRL group. B, HF1 group. C, HF5 group. D, HF10 group.

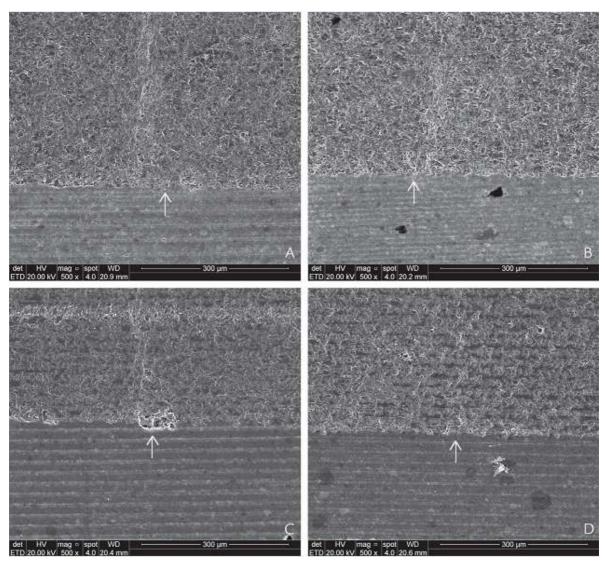


Figure 5. Representative images (original magnification, ×500) of fracture surfaces from crowns subjected to fatigue. A, CTRL group. B, HF1 group. C, HF5 group. D, HF10 group. Radial cracks pointing to fracture origin can be observed in cementation surface under tensile stresses.

TABLES

Table 1. Experimental design.

Group	Surface Treatment
CTRL	Unconditioned control, only silane
HF1	Etching with gel 1% hydrofluoric acid ^a
HF5	Etching with gel 5% hydrofluoric acid ^b
HF10	Etching with gel 10% hydrofluoric acid ^b

^aExperimentally formulated (FGM). ^bCondac Porcelana 5% and 10% (FGM).

Table 2. Mean fatigue failure loads (L_f) and standard deviation (SD) of CAD-CAM feldspathic crowns from staircase tests.

Group	$L_{f}(N) (\pm SD)$
CTRL	$245.0 (\pm 15.1)^{A}$
HF1	$242.5 (\pm 24.7)^{A}$
HF5	$216.7 \ (\pm 22.5)^{\text{B}}$
HF10	255.7 (±53.8) ^A

CAD-CAM, computer-aided design and computer-aided manufacturing. Different superscript letters indicate statistically significant differences (P<.05).

3 ARTIGO 2 – THE EFFECT OF HYDROFLUORIC ACID CONCENTRATION ON THE FATIGUE FAILURE LOAD OF ADHESIVELY CEMENTED FELDSPATHIC CERAMIC DISCS

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The effect of hydrofluoric acid concentration on the fatigue failure load of adhesively cemented feldspathic ceramic discs

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The effect of hydrofluoric acid concentration on the fatigue failure load of adhesively cemented feldspathic ceramic discs

ABSTRACT

Objectives: This study investigated the influence of hydrofluoric acid (HF) etching at different concentrations on the fatigue failure load of adhesively cemented feldspathic ceramic discs (Vita Mark II). Besides, their effect on the micromorphology of ceramic surface was investigated.

Methods: Eighty ceramic discs (ϕ = 10 mm; thickness= 1.5 mm) were cemented to epoxy supporting discs (ϕ = 10 mm; thickness= 2.0 mm) using different surface conditioning methods (n=20): nonetched control (CTRL), or etched for 60 s with different HF concentrations: 1% (HF1), 5% (HF5), or 10% (HF10). All the ceramic discs received a silane application (Monobond Plus). The epoxy discs were etched with 10% HF for 60 s and received a primer coating (Multilink Primer A+B). Adhesively cementation was performed (Multilink Automix), and the assemblies (ceramic discs/epoxy discs) were subjected to cyclic loads in water by a staircase approach (500,000 cycles; 20 Hz; initial load= 290 N; step size= 30 N). Fatigue failure load data were analyzed using 1-way ANOVA and *post-hoc* Tukey's tests (α =.05).

Results: Mean failure load of the HF5 group (255.0 \pm 23.0 N) was significantly lower; HF1 group (301.7 \pm 71.0 N) presented intermediate values, and the highest values were achieved in CTRL (351.7 \pm 13.4 N) and HF10 (341.7 \pm 20.6 N) groups. All the failures were radial cracks starting from the bonding surface.

Significance: In terms of fatigue failure load, etching with 1% and 5% HF had a deleterious effect on the fatigue behavior of an adhesively cemented feldspathic ceramic, while 10% HF had no negative influence.

KEYWORDS: Acid etching. Glass ceramics. Fatigue. Surface treatment. Mechanical cycling.

HIGHLIGHTS

- Hydrofluoric acid (HF) concentration on the fatigue failure load was investigated.
- 5% and 1% HF etching for 60 seconds have demonstrated a deleterious effect.
- 10% HF had no negative influence and seems the recommended protocol for etching.

1. Introduction

Among a wide range of CAD/CAM blocks available to produce monolithic restorations, the feldspathic ceramic Vitablocs Mark II (Vita Zanhfabrik, Bad Säckingen, Germany) is fabricated using fine-structure ceramic powders under industrial sintering process, resulting in good polishing properties, decreased enamel wear, and increased strength due to a nearly pore free ceramic [1]. Also, the fracture resistance of the feldspathic ceramic restorations may be improved with appropriate bonding procedures [2]. To achieve successful bonding, the intaglio surface of these ceramics requires micro-mechanical interlocking by hydrofluoric acid etching, and chemical bonding by a silane coupling agent [3,4].

Even though that adhesive approach is a well-known and recommended method to increase bond strength to feldspathic ceramics, the high toxicity of hydrofluoric acid remains a concern among the clinicians and scientific literature [5] motivating the investigation of lower concentrations of hydrofluoric acid and alternative methods [6-9]. Besides, previous studies showed that mechanical strength of glass-ceramic materials may be negatively influenced by the hydrofluoric acid etching approaches [10-14]. The alterations of the surface flaws (defects' population) as consequence of the etching time and hydrofluoric acid concentration [11] could be the predictive factor of ceramic bulk fractures, mainly if the surface defects are not entirely filled by resin cement [15]. Thereby, only the flexural strength of the ceramic etched by hydrofluoric acid may not exactly reflect the actual strength of all-ceramic restoration [16] since it will be cemented to the tooth. The resin cement could improve the probability of survival of ceramic restorations to a certain extent by healing the cracks [17,18], which depends on the behavior of the resin penetrating the ceramic surface [19].

From the clinical perspective, ceramic restorations are constantly subjected to cyclic loading under wet conditions during chewing function, which should be considered during in

vitro tests, since these conditions decrease the fracture load of restorative materials by slow-crack growth of intrinsic defects [20,21]. Studies about clinically failed glass-ceramic crowns reported that the majority of bulk fractures started from flaws and stresses at the cementation surface [22-24]. From that standpoint, it is important to investigate the influence of the etching protocols in a bonded ceramic surface in attempt to predict the clinical behavior using cyclic loading fatigue tests. Furthermore, limited information is available as to how the use of different hydrofluoric acid concentrations influences the fatigue failure load of adhesively cemented feldspathic ceramic.

Therefore, the current study aimed to evaluate the effect of different hydrofluoric acid concentrations on the fatigue failure loads of feldspathic ceramic discs adhesively bonded. Additionally, micro-morphological evaluations of the ceramic surface in response to the etching protocol and fractographic examinations of the failed specimens were executed. The hypotheses tested were: (1) acid etching would influence the fatigue failure loads compared with nonetched ceramic discs, and (2) different hydrofluoric acid concentrations would promote different fatigue failure loads.

2. Materials and methods

The materials used in this investigation are described in Table 1.

2.1 Specimens preparation and cementation procedure

Feldspathic ceramic blocks (VitaBlocks Mark II for CEREC/inLab, Vita Zahnfabrik, Bad Säckingen, Germany) were shaped into cylinders using a diamond drill (φ= 10 mm; Diamant Boart, Brussels, Belgium) coupled to a bench drill (SBE 1010 Plus, Metabo; Nürtingen, Germany) under refrigeration. The cylinders were cut under water-cooling (Isomet 1000, Buehler, Lake Bluff, United States), resulting in 80 discs with an initial thickness of 1.6 mm. The 'occlusal' surface of the discs was polished with 600-grit SiC polish papers (Ecomet

Polisher, CarbiMet SiC Abrasive Paper grit 600–P1200, Buehler) until the thickness of 1.5 ± 0.1 mm to remove the irregularities of the surface in contact with the piston. The cementation surface was kept 'as-cutting'. Then, the ceramic samples were cleaned (isopropyl alcohol; 5 min) in an ultrasonic bath (Vitasonic, Vita Zahnfabrik).

The epoxy resin discs were shaped into cylinders using a cylindrical diamond drill with an internal diameter of 10 mm in the same way as aforementioned for the ceramic blocks, from plates with 2.0 mm thickness (Epoxy Plate $150 \times 350 \times 2.0$ mm; Carbotec GmbH & Co. KG, Königs Wusterhausen, Germany). A simplified bi-layer setup [25] was designed simulating the restoration of a posterior tooth. On this setup, the ceramic disc represents an occlusal restoration with 10 mm diameter, which is the average surface area of molars according Ferrario et al. [26]; and the epoxy resin disc simulates dentin (ϕ = 10 mm; thickness= 2.0 mm). The bonded two-layer discs had a final thickness of 3.5 mm, which is equivalent to the average thickness from upper pulp wall of the tooth to occlusal surface of the restoration [27-29].

Prior the cementation procedures, the discs were randomly assigned into four groups (n=20) according to the surface conditioning method: nonetched control (CTRL); etched with gel 1%, 5% and 10% hydrofluoric acid (HF1, HF5, and HF10, respectively). The bonding surface of each ceramic disc was etched with one of the different hydrofluoric acid concentrations (1%, 5%, or 10%; FGM, Joinville, Brazil) for 60 s, rinsed with an air-water spray for 30 s, dried, and ultrasonically cleaned in distilled water for 5 min, while the discs of the control group remained nonetched. Subsequently, the silane-based primer (Monobond Plus, Ivoclar Vivadent, Schaan, Liechtenstein) was applied on the bonding surfaces of all ceramic discs scrubbing it on the surfaces for 15 s and then kept to react for 45 s (completing 60 s for the entire procedure), followed by 15 s of air-drying.

The epoxy resin surface was etched with 10% hydrofluoric acid for 60 s, washed for 30 s, and ultrasonically cleaned for 5 min. Multilink Primers A and B (Ivoclar Vivadent) were mixed in a 1:1 ratio, scrubbed on the epoxy surface for 30 s, and dried until a thin film was obtained. After, the ceramic discs were adhesively cemented to the corresponding epoxy discs with resin cement (Multilink Automix, Ivoclar Vivadent). The bonded two-layer discs were seated under a load of 2.5 N (to generate a similar cement thickness), followed by removal of excess cement, and light-activation (Radii-cal, SDI, Bayswater, Australia) for five exposures of 20 s each (one in each direction – 4 positions 0°, 90°, 180°, 270°, and top). All the specimens were stored in distilled water (7 up to 14 days; 37 °C) until the staircase load tests were conducted.

2.2 Fatigue failure load tests

The fatigue tests were conducted in an electric machine (Instron ElectroPuls E3000, Instron Corp, Norwood, United States) with a piston made from epoxy filled with woven glass fibers (φ= 2 mm; NEMA, grade G10; International Paper, Hampton, USA), which was positioned in the center of the ceramic surface (ceramic up, dentin analogue material down). A sheet of polyethylene (0.1 mm thick) was placed between the piston and the ceramic surface to reduce contact stress concentration [30].

Cyclic failure loads (500,000 cycles at 20 Hz) were applied by the staircase approach [31], with amplitudes ranging from a minimum of 10 N to the maximum load to failure. The initial load and the step size were determined based on the results of the monotonic tests from the 10% hydrofluoric acid (HF10) group (n = 3; mean monotonic load for fracture = 483 N). A load of ~60% of the mean monotonic failure load was assumed as the initial load (290 N). A step size of 30 N (~10% of the initial load) was added or subtracted for the next specimen, according to the examination of subsurface crack formation by transillumination. If the tested specimen failed, the next specimen was cycled at a lower load by decreasing one step size. If

the specimen survived to the 500,000 cycles, the subsequent specimen was cycled at a higher load by increasing one step size. According to Collins [31]., it is considered that the test only starts after the first inversion of outcome (survival/fracture); and also that, at least 15 samples should be tested to achieve an accurate measurement after this inversion.

The mean fatigue failure load (L_f) and the standard deviation (s) were calculated based on the data of the least frequent event (survival or failure), using the method described by Collins [31]:

$$\begin{split} L_{\mathbf{i}}f &= L_{\mathbf{i}}f\mathbf{0} + d\left[\left[\sum_{i} in \right]_{\mathbf{i}}i \right] / \left[\sum_{i} n \right]_{\mathbf{i}}i \right] \pm 1/2 \] \\ &= 1,62d \left\{ \left[\left(\sum_{i} n_{i} \sum_{i} i^{2} n_{i} - \left(\left[\sum_{i} in_{i} \right) \right]^{2} \right) / \left(\sum_{i} n_{i} \right)^{2} \right] + 0,029 \right\} \\ &= 1,62d \left\{ \left[\left(\sum_{i} n_{i} \sum_{i} i^{2} n_{i} - \left(\left[\sum_{i} in_{i} \right) \right]^{2} \right) / \left(\sum_{i} n_{i} \right)^{2} \right] + 0,029 \right\} \\ &= 1,62d \left\{ \left[\left(\sum_{i} n_{i} \sum_{i} i^{2} n_{i} - \left(\left[\sum_{i} in_{i} \right) \right]^{2} \right) / \left(\sum_{i} n_{i} \right)^{2} \right] + 0,029 \right\} \\ &= 1,62d \left\{ \left[\left(\sum_{i} n_{i} \sum_{i} i^{2} n_{i} - \left(\left[\sum_{i} in_{i} \right) \right]^{2} \right) / \left(\sum_{i} n_{i} \right)^{2} \right] + 0,029 \right\} \\ &= 1,62d \left\{ \left[\left(\sum_{i} n_{i} \sum_{i} i^{2} n_{i} - \left(\left[\sum_{i} in_{i} \right) \right]^{2} \right) / \left(\sum_{i} n_{i} \right)^{2} \right] + 0,029 \right\} \\ &= 1,62d \left\{ \left[\left(\sum_{i} n_{i} \sum_{i} i^{2} n_{i} - \left(\left[\sum_{i} in_{i} \right) \right]^{2} \right) / \left(\sum_{i} n_{i} \right)^{2} \right] + 0,029 \right\} \\ &= 1,62d \left\{ \left[\left(\sum_{i} n_{i} \sum_{i} i^{2} n_{i} - \left(\left[\sum_{i} in_{i} \right) \right]^{2} \right) / \left(\sum_{i} n_{i} \right)^{2} \right] + 0,029 \right\} \\ &= 1,62d \left\{ \left[\left(\sum_{i} n_{i} \sum_{i} i^{2} n_{i} - \left(\left[\sum_{i} in_{i} \right) \right]^{2} \right) / \left(\sum_{i} n_{i} \right)^{2} \right] + 0,029 \right\} \\ &= 1,62d \left\{ \left[\left(\sum_{i} n_{i} \sum_{i} i^{2} n_{i} - \left(\left[\sum_{i} in_{i} \right) \right]^{2} \right) / \left(\sum_{i} n_{i} \right)^{2} \right] + 0,029 \right\} \\ &= 1,62d \left\{ \left[\left(\sum_{i} n_{i} \sum_{i} i^{2} n_{i} - \left(\left[\sum_{i} in_{i} \right] \right]^{2} \right) / \left(\sum_{i} n_{i} \right)^{2} \right] + 0,029 \right\} \\ &= 1,62d \left\{ \left[\left(\sum_{i} n_{i} \sum_{i} i^{2} n_{i} - \left(\left[\sum_{i} in_{i} \sum_{i} in_{i} \right] \right) / \left(\sum_{i} n_{i} \right)^{2} \right] \right\} \\ &= 1,62d \left\{ \left[\left(\sum_{i} n_{i} \sum_{i} in_{i} - \left(\left[\sum_{i} in_{i} \sum_{i} in_{i} \right] \right) / \left(\sum_{i} n_{i} \right)^{2} \right] \right\} \\ &= 1,62d \left\{ \left[\left(\sum_{i} n_{i} \sum_{i} in_{i} - \left(\sum_{i} in_{i} \sum_{i} in_{i} \right) \right] \right\} \right\} \\ &= 1,62d \left\{ \left[\sum_{i} n_{i} \sum_{i} in_{i} - \left(\sum_{i} in_{i} \sum_{i} in_{i} \right) \right] \right\} \\ &= 1,62d \left\{ \left[\sum_{i} n_{i} \sum_{i} in_{i} + \left(\sum_{i} in_{i} \sum_{i} in_{i} - \left(\sum_{i} in_{i} \sum_{i} in_{i} \right) \right] \right\}$$

where L_{f0} is the lowest load level considered in the analysis, d is the step size and n_i is the number of failures or survivals at the given load level. In Eq. (1), the negative sign is used if the least frequent event is a failure; otherwise the positive sign is used. The lowest load level considered is designated as i = 0, the next level as i = 1, etc. n_i is the number of failures or survivals at a given load level.

2.3 Fractographic analysis

After the fatigue tests, all fractured specimens were analyzed under a light microscope (Stereo Discovery V20; Carl Zeiss, Gottingen, Germany) to determine the region of crack origin. Then, the failed discs were longitudinally sectioned into two halves, perpendicularly to the direction of the radial crack. Representative specimens from each group were analyzed under scanning electron microscopy (SEM; XL 20, FEI Company, GG Eindhoven, The Netherlands).

2.4 Topographic analysis

Topographical analyses were performed by SEM (EVO LS15, Zeiss, Oberkochen, Germany) at different magnifications. The specimens were treated using different conditioning methods, and then sputter coated with a gold-palladium alloy before being examined. Besides, additional specimens were subjected to SEM analysis (Vega3, Tescan, Czech Republic) to verify the bonding interface and the cement penetration into ceramic irregularities created by hydrofluoric acid etching.

2.5 Data analysis

According to Collins [31], only the data from the least frequent event values (failure or survival steps) observed on the fatigue tests should be considered. So, on this sense, the statistical analysis was performed (IBM SPSS Statistics v21 for Windows; IBM Corp) using One-way ANOVA and the post hoc Tukey's test (α =.05).

3. Results

Significant differences for fatigue failure load were found among the evaluated groups (1-way ANOVA, P<.001). On this sense, discs etched by 5% hydrofluoric acid (HF5) presented the lowest mean value in comparison to the CTRL, HF1, and HF10 groups (Table 2). The pattern of runouts (survivals) and failures from the staircase fatigue tests for each group are described in Fig. 1.

The fractographic analysis under a light microscope showed that all failures were radial cracks starting from the cemented surface at the center region, and Hertzian cone cracks were not observed. Representative SEM micrographs of the fracture surfaces are presented in Fig. 2, and also corroborate those assumptions (observed on light microscope).

The SEM analysis revealed a progressive effect of hydrofluoric acid concentration on the ceramic microstructure, indicating that higher concentrations promoted larger and deeper craters and pits (Fig. 3). Fig. 4 shows that the defects (apparently sharper) promoted by low hydrofluoric acid concentrations (1% and 5%) were not entirely filled by the resin cement, while the resin cement penetrated into the irregularities (apparently larger and rounded) introduced by 10% hydrofluoric acid.

4. Discussion

This in vitro study showed a significant effect of hydrofluoric acid concentration on the fatigue failure load of feldspathic ceramic specimens. The first hypothesis that acid etching would influence the fatigue failure loads compared with nonetched ceramic discs was partially accepted, since HF10 and CTRL groups presented statistically similar fatigue failure load values (Table 2). However, a decrease in the fatigue failure load values was observed when ceramic surfaces were etched with 5% and 1% hydrofluoric acid (HF5 < HF1 < HF10). Thus, these findings corroborate the second hypothesis, i.e., different hydrofluoric acid concentrations would promote different fatigue failure loads.

Literature supports that hydrofluoric acid etching mechanism is based on a chemical modification of the ceramic surface, selectively removing the glass matrix, increasing the bonding area (i.e., roughness), and the reactivity to the luting agent (i.e., surface free energy) [32,33]. After etching appropriately the cementation surface of glass ceramics (i.e., producing surface alterations for micromechanical interlocking), and adhesively bonding it to the tooth substrate using low-viscosity resin cements; it may be minimized the influence of critical flaws at this surface [34]. The ability of the resin cement to interpenetrate the ceramic surface defects introduced by etching creates a ceramic-resin composite hybrid layer, which is responsible for the ceramic strengthening effect [19]. Thus, the increase of the fracture resistance of glass ceramics will be in response of an enhanced stress distribution through this

assembly, which decreases the risk of stress concentration on the aforementioned flaws [16,18,35].

In the current investigation, the topographic alterations promoted by 10% hydrofluoric acid resulted in no weakening effect in comparison to the nonetched condition (CTRL), while a negative impact on the fatigue failure load was observed for 1% and 5% concentrations. These findings may be explained by the size and shape of the defects introduced by the different hydrofluoric acid concentrations. In the SEM images, it is possible to observe a progressive effect in response to the increase on acid concentrations (larger and deeper craters) on the ceramic microstructure, and a lesser amount of glassy matrix in all etched surfaces compared with nonetched one. Hence, the largest irregularities, promoted by 10% hydrofluoric acid, enabled an adequate penetration of the resin cement creating a ceramic-resin composite layer, which resulted in a higher fatigue failure load in comparison to the other hydrofluoric acid concentrations (Fig. 4). In regards to the low hydrofluoric acid concentrations (1% and 5%), they probably introduced sharper defects that were not entirely filled by the resin cement, so in this scenario it hypothesizes an ineffective stress distribution (higher stress concentration around the existing defects and leading to premature fracture during smaller loads).

Another important factor to be considered is that hydrofluoric acid etching induces an increased wettability on the adherent (resin cement), in response to an increase in surface area [32]. Increased wettability is associated with a lower contact angle and greater bonding potential among substrates [36]. Venturini et al., [6] tested the same acids used in this study with the same ceramic (Vita Mark II) and observed that hydrofluoric acid etching decreased the contact angle in all etched groups (1, 5 and 10%), on which the lowest mean contact angle value was achieved by 10% hydrofluoric acid. These previous findings also corroborate the

higher filling potential of the cement observed for 10% hydrofluoric acid etching in the current results (Fig. 4).

As aforementioned, acid etching can reduce the stress concentration at existing flaws tips by changing their shape [37]. However, ceramic discs etched with 5% hydrofluoric acid were significantly less resistant than all the other tested groups. This current finding agrees with Venturini et al. [15], who evaluated the influence of hydrofluoric acid concentration on the fatigue failure load of feldspathic ceramic crowns machined by a CAD/CAM system. They stated that HF5 acid had a negative effect on the fatigue loads of Vita Mark II ceramic crowns. In the FE-SEM fractographic images, they observed cement voids at the interface related to the failure origin area. On this scenario, a fraction of the stress at the flaw tip cannot be properly transferred to the resin in these areas with nonhomogeneous penetration of the resin cement (air space), increasing the susceptibility of the ceramic to crack initiation [37]. Thus, our results support the clinical implication proposed by this previous study: the clinical use of 5% hydrofluoric acid (gel) for etching Vita Mark II ceramic should be considered carefully [15].

Also, Venturini et al., [15] noticed that HF1 produced similar values to HF10 and CTRL groups, which is not corroborated by the present findings (HF1 < HF10 and CTRL). Those differences for fatigue behavior of HF1 groups might have been caused by the topographical differences of the ceramic surface from the sample production: they produced the ceramic crowns from the CAD/CAM milling, which leads to a rougher topography in comparison to the methodology of the present study – in vitro cutting processing using a cutting machine. Although the costs of research are reduced with this simplified disc methodology, the mechanical properties might be misinterpreted since machining of partially or fully sintered CAD/CAM ceramics is deleterious to flexural fatigue strength [38]. The topography achieved by CAD/CAM milling is also different from the one achieved by in vitro

laboratorial processing, and that fact could influence on the final mechanical property of the ceramic, so this topographical differences should be considered [39]. It seems that this phenomenon could also be an explanation to the differences between our data and the ones observed previously by Venturini et al., [15]. From the clinical relevance standpoint, studies about the effect of the etching protocols and bonding should consider the simulation of the surface topography promoted by the milling by CAD/CAM system; otherwise an overestimation may be expected if the ceramic surface is not milled by the CAD-CAM system.

Regarding the used materials and test setup, the epoxy supporting material simulates adequately human hydrated dentin in terms of resin cement bond strength and blunt contact elastic behavior as it presents a similar elastic modulus (18 MPa) [40,41]. It is important to highlight that our study used a simplified bi-layer assembly to simulate a monolithic restoration of a posterior first molar (as described by Chen et al., [25]). The main advantage of this assembly is that by controlling the direction of the load application and creating a standardized and fully reproducible scenario, we enable the evaluation of a factor lonely (the effect of etching protocols). This assumption is corroborated by our fractography analysis, which all fractures were radial cracks starting from the cemented surface at the center region, and there was no Hertzian cone crack. Moreover, the use of a personalized piston made from epoxy glass material and a plastic strip may justify the absence of contact damage on the loaded surface [40]. Despite that, this fatigue experiment consists in a laboratorial in vitro study, which cannot fully represent all intraoral conditions, thus containing inherent limitations. Some factors including the direction of the load application such as lateral forces and sliding, anatomical shapes, and hydrolysis of the chemical adhered interface can influence the long-term fracture strength of a ceramic restoration on the clinical intraoral environment. Thus, in vivo researches, to this aim, should be executed in the future.

In conclusion, taking into account the findings depicted by this current fatigue study and the previous adhesion outcomes [15], hydrofluoric acid at 10% concentration remains as the best surface treatment for feldspathic ceramics. Etching with 5% and 1% hydrofluoric acid had a negative effect on the fatigue failure load of adhesively cemented feldspathic discs.

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FIGURES

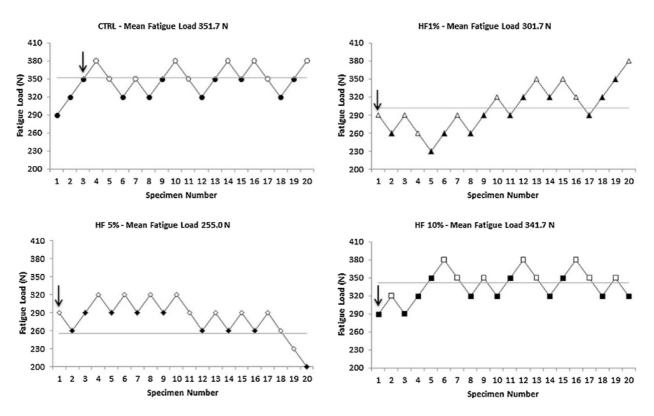


Fig. 1 - Pattern of runouts (survival) and failures for each group (CTRL, HF1, HF5, HF10) observed during wet mechanical cycling (500,000 cycles at 20 Hz). Arrows indicate the load level at which up-and-down characters started. Horizontal lines indicate mean fatigue failure load, filled scorers show runout, and empty scorers are failure.

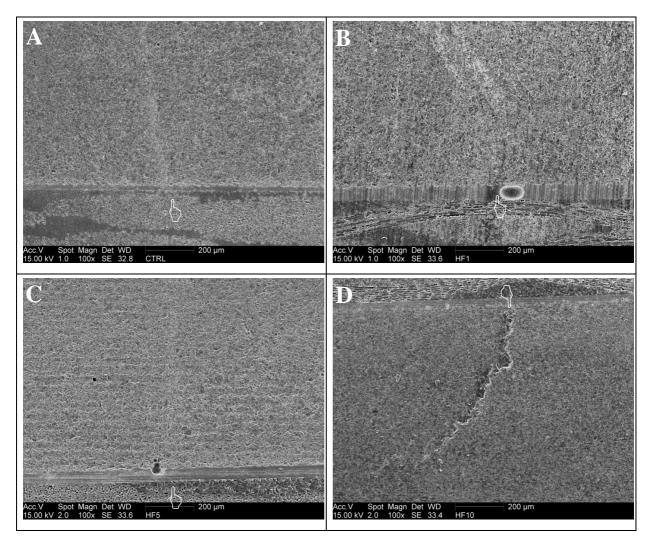


Fig. 2 - Scanning electron microscopy images (original magnification: ×100) of fracture surfaces from discs subjected to fatigue. A, CTRL group. B, HF1 group. C, HF5 group. D, HF10 group. Radial cracks pointing to fracture origin can be observed in cementation surface under tensile stresses.

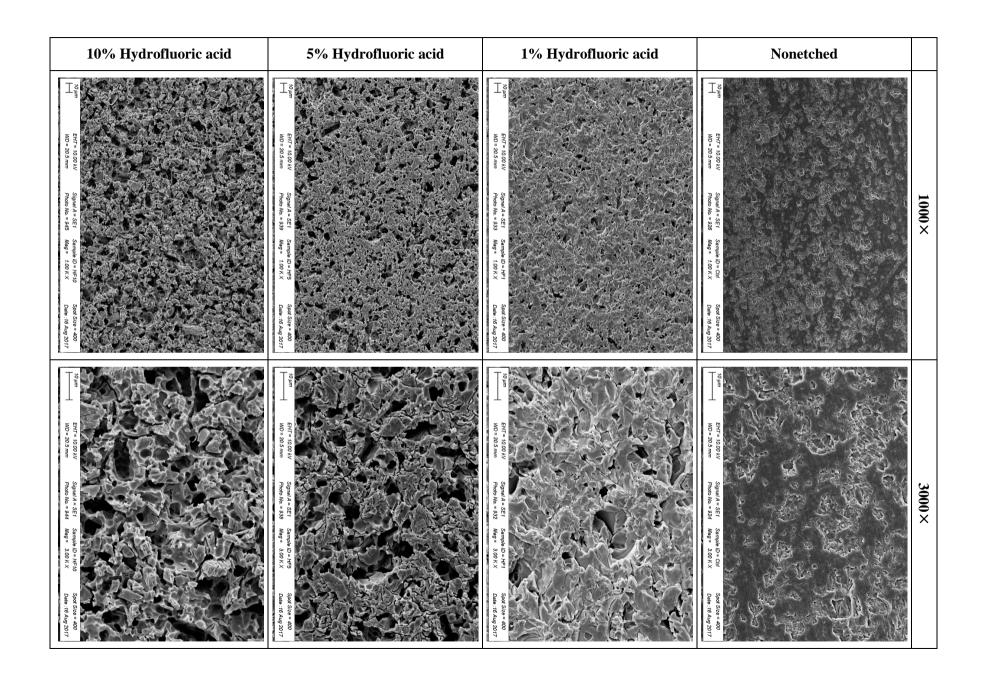
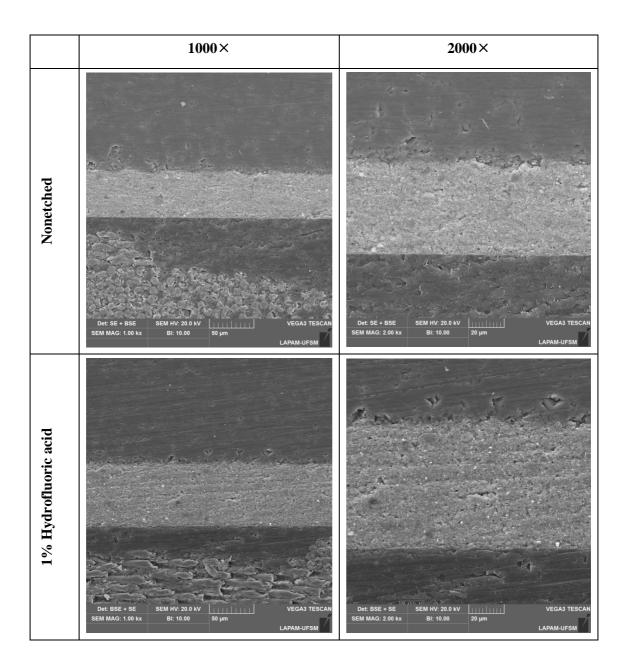


Fig. 3 - Representative SEM micrographs (original magnification, $\times 1000$ and $\times 3000$) of different ceramic surface treatments showing topography pattern alteration generated due to dissolution of the glassy matrix by hydrofluoric acid etching.



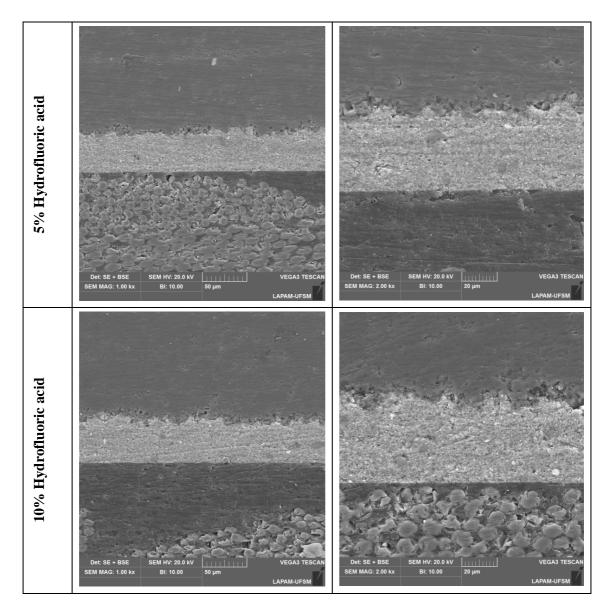


Fig. 4 - SEM images (original magnification, $\times 1000$ and $\times 2000$) of bonding interfaces from tested groups showing cement penetration into ceramic irregularities.

TABLES

Table 1 - Materials used in the study with manufacturer data and composition.

Material	Brand name; Manufacturer (Lot Number)	Composition ^a
Fine-particle feldspar ceramic	VITABLOCS Mark II; Vita Zahnfabrik (LOT 28650)	Al ₂ O ₃ , SiO ₂ , K ₂ O, Na ₂ O, CaO, TiO ₂ , other oxides
Epoxy resin plate	Epoxy platte 150x350x2,0 mm; Carbotec GmbH & Co. KG, Germany	Epoxy resin
Dual-cured resin cement	Multilink Automix; Ivoclar Vivadent AG, Liechtenstein (LOT U19980)	Dimethacrylates, HEMA, barium glass filler, ytterbium trifluoride, highly dispersed silica, catalysts and stabilizer, pigments
Primer	Multilink Primer A and Primer B; Ivoclar Vivadent AG, Liechtenstein (LOT U22990)	Primer A: water, initiators; Primer B: phosphonic acid acrylate, hydroxyethyl methacrylate, methacrylate mod. polyacrylic acid, stabiliser
Silane	Monobond Plus; Ivoclar Vivadent AG, Liechtenstein (LOT U25466) Alcohol solution of silane methacrylate, phosphoric acid methacrylate, and sulphide methacrylate	
Hydrofluoric acid	Experimentally formulated 1% Condac Porcelana 5% Condac Porcelana 10% FGM, Brazil (LOT 030216)	Hydrofluoric acid at 1%, 5%, and 10%, water, thickener, surfactant, and coloring

^aThe chemical compositions are described according to the manufacturers' information.

 $\begin{tabular}{ll} \textbf{Table 2 -} Mean fatigue failure loads (L_f) and standard deviation (SD) of tested groups from staircase tests. \end{tabular}$

Group	$L_{f}(N) (\pm SD)$
CTRL	$351.7 (\pm 13.4)^{A}$
HF1	$301.7 (\pm 71.0)^{B}$
HF5	$255.0 (\pm 23.0)^{C}$
HF10	$341.7 (\pm 20.6)^{A}$

Different letters indicate statistically significant differences (P<.05).

4 DISCUSSÃO

A união entre a estrutura dental e as restaurações cerâmicas indiretas é um fator imprescindível para o sucesso e longevidade das restaurações cerâmicas (MALAMENT; SOCRANSKY; 2001). Embora o condicionamento com ácido fluorídrico seja necessário para promover o embricamento micro mecânico com os materiais resinosos e a estrutura dental, pouco se sabe sobre os efeitos que as irregularidades criadas por esse ácido podem provocar nas propriedades mecânicas das cerâmicas submetidas a cargas cíclicas em ambiente oral úmido. O condicionamento ácido deveria, ao mesmo tempo, criar uma topografia de superfície suficientemente irregular para uma união adequada com o cimento resinoso sem causar o enfraquecimento da estrutura cerâmica. Neste sentido, o uso de concentrações mais baixas de ácido fluorídrico tem sido considerado juntamente ao fato desse ácido ser perigoso e particularmente agressivo aos tecidos devido à alta toxicidade (OZCAN; ALLAHBEICKARAGHI; DUNDAR, 2012).

Considerando que o tratamento de superfície com ácido fluorídrico pode criar zonas de fragilidade nas restaurações cerâmicas, as quais são submetidas a cargas cíclicas em ambiente oral, uma trinca poderá iniciar e propagar-se para a fratura catastrófica do material. Nesse sentido, os ensaios de fadiga têm se colocado como uma alternativa aos testes monotônicos de resistência flexural, pois se aproximam mais da realidade clínica que os materiais restauradores são submetidos.

Assim, a realização dos dois artigos que compõem esta tese foi impulsionada pela necessidade de prever de maneira mais confiável o comportamento mecânico à fadiga da superfície cerâmica após os procedimentos de condicionamento com ácido fluorídrico e cimentação. Diante disso, objetivou-se avaliar a influência de diferentes concentrações de ácido fluorídrico no condicionamento de espécimes de cerâmica feldspática na forma de discos e de coroas usinadas pelo sistema CAD/CAM, os quais foram cimentados adesivamente a um material análogo a dentina, e submetidos a cargas cíclicas na presença de água.

A partir da evidência de que o condicionamento com ácido fluorídrico tem um efeito de enfraquecimento na resistência de cerâmicas vítreas (ADDISON; FLEMING, 2004; ADDISON; MARQUIS; FLEMING, 2007b; HOOSHMAND; PARVIZI; KESHVAD, 2008; ZOGHEIB, 2011; VENTURINI et al., 2015b), uma das hipóteses testadas foi de que o condicionamento ácido influenciaria negativamente as cargas para falha em fadiga em

comparação aos espécimes cerâmicos não condicionados. Entretanto, as coroas não condicionadas (CTRL) e as coroas condicionadas com ácido fluorídrico 1% e 10% (HF1 e HF10) apresentaram valores de carga para falha em fadiga estatisticamente similares, assim como os discos não condicionados e os discos condicionados com HF10. A explicação para esses achados pode estar no procedimento de cimentação mediante a capacidade do cimento resinoso em penetrar nos defeitos da superfície cerâmica e criar uma camada híbrida cerâmica-resina, que é responsável pelo efeito de reforço cerâmico (ADDISON; MARQUIS; FLEMING, 2007a). Investigações prévias já haviam relatado uma influência positiva da aplicação de cimento resinoso na resistência flexural de cerâmicas vítreas (ADDISON; MARQUIS; FLEMING, 2007a; POSRITONG et al., 2013). Além disso, o potencial de penetração do cimento resinoso está diretamente associado a uma maior molhabilidade do aderente, menor ângulo de contato e maior potencial de ligação entre os substratos (AMARAL et al., 2011). Logo, a justificativa para a adequada e homogênea penetração do cimento resinoso nas irregularidades da superfície cerâmica condicionada com ácido fluorídrico 10% deve-se ao maior tamanho e formato arredondado das irregularidades criadas pelo HF10 juntamente ao fato desse ácido ter apresentado um menor ângulo de contato comparado às outras concentrações em estudo prévio (VENTURINI et al., 2015a).

Em relação à influência das diferentes concentrações de ácido fluorídrico, as cargas médias para falha em fadiga foram significativamente inferiores quando as superfícies cerâmicas foram condicionadas com ácido fluorídrico 5% (HF5) tanto nas coroas como nos discos testados. As imagens realizadas em microscópio eletrônico de varredura mostram que o cimento resinoso não conseguiu penetrar completamente nas irregularidades mais pontiagudas criadas pelo ácido fluorídrico 5%, sendo observados vazios de cimento na interface relacionados à área de origem da falha. Nesse cenário, a presença de falhas e vazios de cimento ao longo da superfície de cimentação faz com que as tensões internas se concentrem distribuídas nessa região não possam ser para conjunto cerâmica/cimento/dente (ANUSAVICE; HOJJATIE, 1992), o que aumenta a suscetibilidade da cerâmica ao início da trinca e, consequentemente, leva à falha prematura durante cargas baixas.

Como mencionado anteriormente, as coroas cerâmicas condicionadas com ácido fluorídrico 1% apresentaram cargas para falha em fadiga similares as coroas não condicionadas e as condicionadas com ácido fluorídrico 10% (HF1 = CTRL e HF10), diferentemente ao observado nos discos tratados com a concentração de 1% (HF1 < CTRL e HF10). Uma explicação plausível para a diferença entre o comportamento de fadiga das

coroas e discos condicionados com HF1 é a topografia da superfície cerâmica decorrente do processo de usinagem das coroas pelo sistema CAD/CAM prévio ao condicionamento. A usinagem dos blocos cerâmicos leva a uma topografia mais rugosa comparada à metodologia do segundo artigo, no qual os discos foram apenas seccionados em uma máquina de corte. Embora os custos da pesquisa sejam reduzidos com essa metodologia de disco simplificada e os resultados sejam praticamente os mesmos entre os estudos (HF5 < CTRL e HF10), as diferenças topográficas devem ser consideradas visto que a usinagem de blocos cerâmicos para CAD/CAM parcialmente ou totalmente sinterizados afeta negativamente a resistência à fadiga flexural (FRAGA et al., 2017). Assim, sugere-se que estudos futuros sobre o efeito de diferentes protocolos de condicionamento simulem a topografia de superfície promovida pela usinagem por meio do sistema CAD/CAM.

De acordo com a fractografia das coroas e discos testados, todas as falhas ocorreram como trincas radiais a partir da superfície de cimentação, o que se aproxima dos estudos que avaliaram coroas cerâmicas que falharam clinicamente (KELLY et al., 1990; THOMPSON et al., 1994), visto que é nesta superfície que se concentram grande parte das tensões de tração responsáveis pelo início da falha (KELLY, 1999). Ademais, o uso de um pistão de resina epóxi com fibra de vidro e de uma tira plástica entre o pistão e o espécime durante o teste pode justificar a ausência de danos de contato na superfície cerâmica (KELLY et al., 2010).

Os estudos *in vitro* que compõem esta tese não simularam completamente todas as condições clínicas, e, desta maneira, contêm limitações inerentes. Nesse sentido, os espécimes testados receberam aplicação de cargas cíclicas apenas no sentido axial, sendo que as forças laterais e de deslizamento, que ocorrem clinicamente durante a mastigação, não foram simuladas. Além disso, o tempo de armazenamento (7 – 14 dias) pode ter sido insuficiente para promover a hidrólise da interface química e interferir na durabilidade da resistência adesiva da restauração cerâmica. Desta maneira, a retenção micromecânica mínima promovida pelo condicionamento com ácido fluorídrico 1%, ou apenas a união química decorrente da aplicação do silano na cerâmica não condicionada, pode ter sido insuficiente para uma resistência de união estável ao longo do tempo. Assim, ensaios clínicos randomizados e investigações adicionais devem ser conduzidos para confirmar os achados destes estudos clinicamente.

5 CONCLUSÃO

A partir dos dois artigos apresentados nesta tese, pode-se concluir que o condicionamento com ácido fluorídrico a 5% reduziu as cargas para falha em fadiga tanto das coroas como dos discos de cerâmica feldspática cimentados adesivamente e, portanto, o uso clínico da concentração de 5% do ácido investigado deve ser considerado cuidadosamente para o condicionamento dessa cerâmica. Assim, com base nos achados desta tese e da necessidade de adesão micromecânica entre os substratos, o condicionamento com ácido fluorídrico a 10% é o tratamento de superfície recomendado para a cerâmica testada visto que não apresentou efeito deletério nas cargas para falha em fadiga em ambos os estudos.

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ANEXO A – NORMAS PARA PUBLICAÇÃO NO PERIÓDICO THE JOURNAL OF PROSTHETIC DENTISTRY

Article Types

Articles are classified as one of the following: research/clinical science article, clinical report, technique article, systematic review, or tip from our readers. Required sections for each type of article are listed in the order in which they should be presented.

Research and Education/Clinical Research

The research report should be no longer than 10-12 double-spaced, typed pages and be accompanied by no more than 12 high-quality illustrations. Avoid the use of outline form (numbered and/or bulleted sentences or paragraphs). The text should be written in complete sentences and paragraph form. *Abstract* (approximately 400 words): Create a structured abstract with the following subsections: Statement of Problem, Purpose, Material and Methods, Results, and Conclusions. The abstract should contain enough detail to describe the experimental design and variables. Sample size, controls, method of measurement, standardization, examiner reliability, and statistical method used with associated level of significance should be described in the Material and Methods section. Actual values should be provided in the Results section.

Clinical Implications: In 2-4 sentences, describe the impact of the study results on clinical practice.

Introduction: Explain the problem completely and accurately. Summarize relevant literature, and identify any bias in previous studies. Clearly state the objective of the study and the research hypothesis at the end of the Introduction. Please note that, for a thorough review of the literature, most (if not all references) should first be cited in the Introduction and/or Material and Methods section.

Material and Methods: In the initial paragraph, provide an overview of the experiment. Provide complete manufacturing information for all products and instruments used, either in parentheses or in a table. Describe what was measured, how it was measured, and the units of measure. List criteria for quantitative judgment. Describe the experimental design and variables, including defined criteria to control variables, standardization of testing, allocation of specimens/subjects to groups (specify method of randomization), total sample size, controls, calibration of examiners, and reliability of instruments and examiners. State how sample sizes were determined (such as with power analysis). Avoid the use of group numbers to indicate groups. Instead, use codes or abbreviations that will more clearly indicate the characteristics of the groups and will therefore be more meaningful for the reader. Statistical tests and associated significance levels should be described at the end of this section.

Results: Report the results accurately and briefly, in the same order as the testing was described in the Material and Methods section. For extensive listings, present data in tabular or graphic form to help the reader. For a 1-way ANOVA report of, F and P values in the appropriate location in the text. For all other ANOVAs, per guidelines, provide the ANOVA table(s). Describe the most significant findings and trends. Text, tables, and figures should not repeat each other. Results noted as significant must be validated by actual data and P values.

Discussion: Discuss the results of the study in relation to the hypothesis and to relevant literature. The Discussion section should begin by stating whether or not the data support rejecting the stated null hypothesis. If the results do not agree with other studies and/or with accepted opinions, state how and why the results differ. Agreement with other studies should also be stated. Identify the limitations of the present study and suggest areas for future research.

Conclusions: Concisely list conclusions that may be drawn from the research; do not simply restate the results. The conclusions must be pertinent to the objectives and justified by the data. In most situations, the conclusions are true for only the population of the experiment. All statements reported as conclusions should be accompanied by statistical analyses.

References: See Reference Guidelines and Sample References page.

Tables: See Table Guidelines.

Illustrations: See Figure Submission and Sample Figures page.

Clinical Report

The clinical report describes the author's methods for meeting a patient treatment challenge. It should be no longer than 4 to 5 double-spaced, pages and be accompanied by no more than 8 high-quality illustrations. In some situations, the Editor may approve the publication of additional figures if they contribute significantly to the manuscript.

Abstract: Provide a short, nonstructured, 1-paragraph abstract that briefly summarizes the problem encountered and treatment administered.

Introduction: Summarize literature relevant to the problem encountered. Include references to standard treatments and protocols. Please note that most, if not all, references should first be cited in the Introduction and/or Clinical Report section.

Clinical Report: Describe the patient, the problem with which he/she presented, and any relevant medical or dental background. Describe the various treatment options and the reasons for selection of the chosen treatment. Fully describe the treatment rendered, the length of the follow-up period, and any improvements noted as a result of treatment. This section should be written in past tense and in paragraph form.

Discussion: Comment on the advantages and disadvantages of the chosen treatment and describe any contraindications for it. If the text will only be repetitive of previous sections, omit the Discussion.

Summary: Briefly summarize the patient treatment.

References: See Reference Guidelines and Sample References page.

Illustrations: See Figure Submission and Sample Figures page.

Dental Technique

The dental technique article presents, in a step-by-step format, a unique procedure helpful to dental professionals. It should be no longer than 4 to 5 double-spaced, typed pages and be accompanied by no more than 8 high-quality illustrations. In some situations, the Editor may approve the publication of additional figures if they contribute significantly to the manuscript.

Abstract: Provide a short, nonstructured, 1-paragraph abstract that briefly summarizes the technique.

Introduction: Summarize relevant literature. Include references to standard methods and protocols. Please note that most, if not all, references should first be cited in the Introduction and/or Technique section.

Technique: In a numbered, step-by-step format, describe each step of the technique. The text should be written in command rather than descriptive form ("Survey the diagnostic cast" rather than "The diagnostic cast is surveyed.") Include citations for the accompanying illustrations.

Discussion: Comment on the advantages and disadvantages of the technique, indicate the situations to which it may be applied, and describe any contraindications for its use. Avoid excessive claims of effectiveness. If the text will only be repetitive of previous sections, omit the Discussion.

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[2] W. Strunk Jr., E.B. White, The Elements of Style, fourth ed., Longman, New York, 2000. Reference to a chapter in an edited book:

[3] G.R. Mettam, L.B. Adams, How to prepare an electronic version of your article, in: B.S. Jones, R.Z.

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